

# MODELLING OF FOCAL ADHESIONS CONSIDERABLY AFFECTS THE PREDICTED INTRACELLULAR STRAIN FIELD



Laura Dubuis<sup>1</sup>, Neil H. Davies<sup>2</sup>, Jason Green<sup>2,5</sup>, Thomas Franz<sup>1,3,4,5</sup>

<sup>1</sup> Division of Biomedical Engineering, Department of Human Biology, <sup>2</sup> Cardiovascular Research Unit, <sup>3</sup> Research Office,

<sup>4</sup> Centre for Research in Computational and Applied Mechanics, University of Cape Town, Observatory, South Africa.

<sup>5</sup> Centre for High Performance Computing, Rosebank, South Africa. <sup>6</sup> Wake Forest Institute for Regenerative Medicine, Wake Forest University, Winston-Salem, USA

## 1. Context

### Myocardial Infarction (heart attack)

→ Death of a part of the myocardium

1. Loss of contractile properties
2. Tissue stiffness and thickness modification
3. Remodelling

High risk of heart failure!

### Remodelling prevention

→ Emerging therapy: Injection of hydrogel into the infarct

Hydrogel =

- 99 % water
- Polymer

Stem cells

### Questions

What is the effect of:

- the **focal adhesion (FA)** modelling
- the **structural stiffness** of the extracellular matrix (ECM) on the strain field?

### Mechanotransduction

**Mechanical stresses**

- Hydrostatic pressure
- Shear stress
- Stretching
- ...

**Biological response**

- Remodelling
- Cell proliferation
- Differentiation
- Gene expression
- Protein synthesis
- ...

## 2. Methods

### Geometry

Z-stack from confocal microscope

Segmentation + smoothing

1

Segmented image

3D generation

2

3D volume

Meshing

3

Mesh

### Mechanical properties

Component	Constitutive law	Parameters
Cytosol [1]	Neo-Hookean	$c_{10} = 0.5$ kPa
Nucleus [4]		$\kappa = 9.7$ kPa
		$c_{10} = 0.8$ kPa
		$\kappa = 16.4$ kPa
Membrane	Hooke (linear)	$E = 0.1-100$ kPa
		$\nu = 0.47$

### Boundary conditions

#### Step 1: Contact initiation

- Cell: vertical displacement till contact
- Membrane: fixed at its boundaries

#### Step 2: Tie constraint

- Cell: glued to the membrane at the FAs
- Membrane: fixed at its boundaries

#### Step 3: Stretching

- Cell: glued to the membrane at the FAs
- Membrane: stretched along the x axis

### Three models of cell-substrate contact

Uneven with focal adhesions (UFA)

- Bottom of the cell is uneven (following the microscope image).
- FA are located at the contact areas with the ECM.

Even with focal adhesions (EFA)

- Bottom of the cell is even (smoothed).
- FA are located at the same location as UFA.

Even with large contact (ELC)

- Bottom of the cell is even (smoothed).
- Large contact area between the bottom and the ECM.

## 3. Results

### Strain field in the cell for the different models with the same structural stiffness of extracellular matrix

Structural stiffness = Young modulus × thickness =  $0.01 \times 0.14 = 0.0014$  MPa.mm

### Effect of the structural stiffness of the ECM on the global stretch of the cell

Global stretch =  $\frac{L-L_0}{L_0}$

## 4. Conclusion

- ✓ **Global strain** of the cell depends of structural properties of the extra-cellular matrix.
  - The stiffness of the ECM affects the mechanical response of the cell.
- ✓ **Strain field** in the cell depends on the FA position/surface and is non-homogeneous.
  - Location of FAs have a significant effect on the strain field.

## References

- [1] Breuls *et al.*, J. Biomech. Eng. 2002, 124: 198–207.
- [2] Breuls *et al.*, Open. Orthop J. 2008; 2: 103–109.
- [3] Ferko *et al.*, Ann. Biomed. Eng. 2007, 35: 2008–223.
- [4] Jean *et al.*, J. Biomech. Eng. 2005, 127: 194 – 200.
- [5] Ofek *et al.*, J. Biomech. 2009, 42: 873–878.
- [6] Or-Tzadikario *et al.*, J. Biomech. 2011, 44: 567–573.
- [7] Slomka *et al.*, J. Biomech. 2010, 43: 1806–1816.

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